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Dkt. 1141/73790

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Listing of Claims

The following listing of claims will replace all prior versions, and listings, of claims in the subject application:

1. (currently amended) An X-ray tomograph comprising:

a radiation source and a radiation detector arranged opposite to each other, between which a bed with an examinee placed thereon is provided, said radiation source and radiation detector turning around said bed which ~~can be moved~~ is configured to move with respect to a go-around axis, radiation irradiated from said radiation source and passing through the examinee being detected using said radiation detector and being converted to projection data; and

reconfiguration means for creating a three-dimensional tomographic image in a region in concern of the ~~object~~ examinee from the ~~detected~~ projection data,

wherein said reconfiguration means determines, for each voxel, a projection data phase range as an angle between 180 and 360 degrees from projection data obtained at a spiral orbit scan so that a difference in absolute values of cone angles at both ends of the projection data phase range used is ~~reduced~~ minimized, superimposes a reconfiguration filter, assigns weights to data of ~~[[the]]~~ a same phase or opposite phase for each phase for the projection data phase range, and three-dimension back projects the filter-processed projection data over said projection data phase range determined for each voxel along ~~[[the]]~~ an irradiation trace of ~~[[the]]~~ a radiation beam.

Claim 2 (canceled).

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3. (previously presented) The X-ray tomograph according to claim 1, wherein the projection data phase range used is determined so as to be the same phase range for each voxel.

Claim 4 (canceled).

5. (currently amended) The X-ray tomograph according to any one of claims ~~1, 3 and 4~~ 1 and 3, wherein projection data ~~[[whose]]~~ for a number of images taken per rotation ~~that~~ is a multiple of ~~[[the]]~~ a number of sides C of a rectangle or hexagon is acquired, and said reconfiguration means comprises back projection means for superimposing said reconfiguration filter on ~~[[this]]~~ the acquired projection data, grouping data at ~~[[the]]~~ a same channel position and having projection phases in ~~[[the]]~~ a go-around direction shifting by $2N\pi/C$ ($N=1, 2, 3, \dots$) radians at a time and performing back projection to a square image array group by group.

6. (currently amended) The X-ray tomograph according to any one of claims ~~1, 3 and 4~~ 1 and 3, wherein said reconfiguration means converts the projection data obtained to data including fan beam data and parallel beam data ~~[[whose]]~~ for a number of images taken per rotation ~~that~~ is a multiple of ~~[[the]]~~ a number of sides C of a rectangle or hexagon, superimposes the reconfiguration filter on ~~this projection~~ the converted data, groups data at ~~[[the]]~~ a same channel position and having projection phases in ~~[[the]]~~ a go-around direction shifting by $2N\pi/C$ ($N=1, 2, 3, \dots$) radians at a time and performs back projection to a square image array group by group.

7. (currently amended) The X-ray tomograph according to claim 1, ~~wherein~~ further

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comprising associating means ~~is provided~~ for associating ~~pixel intervals~~ voxel pitch in ~~[[the]]~~ a body axis direction with ~~[[the]]~~ a relative moving speed between the ~~object~~ examinee and said radiation source in ~~[[the]]~~ a go-around axis direction.

8. (currently amended) The X-ray tomograph according to claim 7, wherein said associating means is constructed so that ~~[[the]]~~ a relationship between ~~pixel interval~~ voxel pitch ~~rpitch~~ in the body axis direction of a square image and the relative moving speed in the go-around axis direction of the ~~object~~ examinee and said radiation source is expressed by $2 \cdot N \cdot \text{rpitch}$ ($N=1, 2, 3 \dots$).

9. (previously presented) The X-ray tomograph according to claim 8, wherein at the phase of $N\pi$ ($N=1, 2, 3, \dots$) radians of the radiation source, the position on the radiation detector at which the beam passing through a voxel I (x, y, Z) whose body axis direction position is Z millimeters intersects and the position on the radiation detector at which the beam passing through a voxel I ($-x, -y, NJ/2+Z$) whose body axis direction position is $N \cdot J/2 + Z$ millimeters intersects are the same.

Claims 10-14 (canceled).